

Changes in Plasticity Across the Lifespan: Cause of Disease and Target for Intervention

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Abstract

We conceptualize brain plasticity as an intrinsic property of the nervous system enabling rapid adaptation in response to changes in an organism's internal and external environment. In prenatal and early postnatal development, plasticity allows for the formation of organized nervous system circuitry and the establishment of functional networks. As the individual is exposed to various sensory stimuli in the environment, brain plasticity allows for functional and structural adaptation and underlies learning and memory. We argue that the mechanisms of plasticity change over the lifespan with different slopes of change in different individuals. These changes play a key role in the clinical phenotype of neurodevelopmental disorders like autism and schizophrenia and neurodegenerative disorders such as Alzheimer's disease. Altered plasticity not only can trigger maladaptive cascades and can be the cause of deficits and disability but also offers opportunities for novel therapeutic interventions. In this chapter, we discuss the importance of brain plasticity across the lifespan and how neuroplasticity-based therapies offer promise for disorders with otherwise limited effective treatment.

Keywords

plasticity, aging, lifespan, transcranial magnetic stimulation, autism spectrum disorders, schizophrenia, Alzheimer's disease

1 INTRODUCTION

Brain plasticity is an intrinsic property of the nervous system that allows an individual to adapt to a rapidly changing environment through strengthening, weakening, pruning, or adding of synaptic connections and by promoting neurogenesis

(Feldman, 2009; Pascual-Leone et al., 2005). Plasticity might be conceptualized as the balanced interplay of mechanisms promoting change and those promoting stability (homeostatic plasticity). At the synaptic level, this plays out, for example, in the balance of long-term potentiation (LTP) strengthening connections between presynaptic and postsynaptic neurons (Bliss and Gardner-Medwin, 1973) and long-term depression (LTD) weakening them (Bear and Abraham, 1996). The propensity of a synapse to undergo potentiation or depression relies on the influence of a number of molecular mechanisms (Kandel, 2001) and the current state of the synapse (whether it has undergone a plastic change in the recent past, the so-called metaplastic influences (Abraham, 2008; Mockett and Hulme, 2008)).

The molecular mechanisms responsible for plasticity are complex involving multiple cascades eventually culminating in functional and structural changes. Many models of plasticity propose the involvement of the NMDA receptor that, depending on the timing and degree of depolarization of the postsynaptic cell, leads to subsequent synaptic LTP or LTD (e.g., Daw et al., 1993; Malenka and Nicoll, 1993; McBain and Mayer, 1994). This process is kept in check by regulatory forms of plasticity to avoid a situation whereby certain cells never fire and others fire constantly. These feedback mechanisms include homeostatic synaptic scaling, whereby uniform increases or decreases in network activity over several hours or days lead to an opposing increase or decrease in excitatory synaptic strength (Turrigiano and Nelson, 2004). Metaplasticity is another feedback mechanism, where experience-dependent alterations in inhibitory tone, dendritic excitability, and NMDA receptor function alter the ability of future stimuli to drive LTP and LTD (Abraham and Bear, 1996). Plasticity at the synaptic level can be studied using *in vitro* techniques or *in vivo* in animal models. These changes at the synaptic level lead to the development and maintenance of neural circuitry.

Characterization of plasticity in humans is possible. The consequences of brain plasticity can be studied as changes in functional activity and anatomical connectivity using neuroimaging and neurophysiological techniques and as changes in behavior captured by measures of learning, memory, and adaptation. For example, brain imaging studies using structural and functional magnetic resonance imaging (MRI) and diffusion tensor imaging (DTI) have provided evidence of circuit modification suggestive of plastic changes (Guye et al., 2008; Voss and Schiff, 2009). These circuit modifications are indirect measures of what is happening at the cellular level.

Cross-sectional anatomical MRI studies have consistently identified age-associated morphometric brain changes encompassing regional cortical thinning, volumetric subcortical reductions, and ventricular enlargement (e.g., Fjell et al., 2009; Walhovd et al., 2005, 2009). Longitudinal studies have demonstrated annual atrophy rates for brain volume, hippocampus and entorhinal cortex (e.g., Fotenos et al., 2005; Scahill et al., 2003), and atrophy in cortical brain regions over different periods of time (Driscoll et al., 2009; Raz et al., 2005). Cortical thickness decreases over the lifespan are estimated at 0.5% a year (Thompson et al., 2007). These changes affect different neural systems differently: motor and visual cortices show regional thinning, whereas nonlimbic temporal regions and parietal areas are

relatively spared in normal aging (Raz et al., 2004; Salat et al., 2004). Furthermore, DTI can reveal structural changes in white matter structure (myelination) and connectivity. For example, DTI has demonstrated that white matter connections, largely in frontostriatal areas, have reduced myelination as age increases (Salat et al., 2005).

Functional MRI can reveal changes in activation of brain circuits across the age span. One example of this is a reduction in prefrontal hemispheric asymmetry in elderly individuals, referred to as the HAROLD (hemispheric asymmetry reduction in older adults) model (Cabeza et al., 2002). According to the HAROLD model, the older brain displays less localizable and more bilateral activation during certain cognitive tasks. A second pattern is a shift in evoked neural activity from posterior to anterior cortex, a model referred to by Davis et al. as PASA (posterior–anterior shift in aging) (Davis et al., 2008). The PASA model posits that the aging brain is more likely to recruit prefrontal, rather than occipitotemporal, cortex in the service of task execution. In addition to life-span changes in task-related brain activation patterns, resting-state fMRI is revealing age-related differences in the functional connectivity across large-scale brain networks. One such large-scale brain functional network, the default mode network (DMN), has been shown to undergo notable modifications with advancing age in health and disease (Buckner et al., 2008). Older individuals reportedly exhibit significantly lower DMN activity in the posterior cingulate and a tendency toward lower activity in all other DMN regions as compared to younger subjects (Koch et al., 2010). Functional connectivity within the DMN also seems to be reduced in older adults (Grady et al., 2010). During performance of a working memory task, the pattern of deactivation of the DMN also seems to be affected by aging, with older individuals showing not only decreased connectivity but also decreased ability to suppress low-frequency oscillations of the DMN (Sambataro et al., 2010). Age-specific changes in activation and connectivity are also seen in the task-positive network (TPN), though the functional significance of this remains uncertain (Grady et al., 2010; Sambataro et al., 2010). During memory encoding and recognition, age-related changes appear to occur mainly in the long-range connections with widespread reductions associated with aging in the frontotemporal and temporoparietal regions and a few age-related increases in the posterior parietal regions (Wang et al., 2010). During developmental years, children and young adults appear to have similar patterns of functionally connected regions but with differences in the size of functionally connected regions and in the strength of functional connectivity between brain regions (Jolles et al., 2011).

Though useful for understanding the consequences of plasticity at the circuit level, brain imaging does not directly probe plasticity but rather reveals its consequences. Direct measures of circuit-level plasticity in humans *in vivo* can be obtained using novel transcranial magnetic stimulation (TMS) paradigms (Huang et al., 2005; Huerta and Volpe, 2009; Thickbroom, 2007; Ziemann, 2004). TMS is a noninvasive way to induce, measure, and modify local and network plasticity, and a number of experimental TMS measures of brain plasticity have been introduced. Single-pulse TMS combined with EMG, EEG, fMRI, or other brain imaging methods can be used to quantify cortical reactivity before and following a given intervention

(Pascual-Leone et al., 2011). TMS can provide a controlled and quantifiable input that can be matched across individuals of different ages. Comparison of TMS measures of cortical reactivity before and after an intervention may thus provide an index of brain plasticity in response to said intervention. When the intervention itself involves TMS (as in paired associative stimulation (PAS) or repetitive (r)TMS protocols), it is possible to assess the efficacy of the mechanisms of plasticity in a defined cortical brain region in humans *in vivo*. PAS builds on the Hebbian principle of spike timing-dependent synaptic plasticity (Classen et al., 2004). In its most common form, PAS involves repeated pairing of median nerve electric stimulation with timed TMS over the contralateral primary motor cortex. In this form, PAS has been shown to modulate the excitability of the motor system in either the positive (with an ISI of 25 ms) or negative (with an ISI of 10 ms) direction (Classen et al., 2004). Repetitive TMS (rTMS) consists in the application of a train of TMS pulses of the same intensity to a single brain area at a given frequency that can range from 1 to 20 or more stimuli per second (Pascual-Leone et al., 1994). Such a train of rTMS can induce a modulation of cortical excitability beyond the duration of the train itself. Depending on the stimulation parameters, particularly frequency and pattern of stimulation, cortical reactivity is potentiated or depressed (Pascual-Leone et al., 1994). In general, a continuous train of lower frequencies of rTMS, in the 1 Hz range, leads to a transient suppression of excitability in the targeted cortical area, while bursts of high-frequency stimulation (≥ 5 Hz) lead to a temporary increase in cortical reactivity (Kobayashi and Pascual-Leone, 2003). Patterned bursting protocols have also been developed that mimic paradigms used to assess synaptic plasticity in animal models (Huang et al., 2005, 2008). Specifically, theta burst stimulation (TBS) involves application of three bursts of 50 Hz rTMS repeated every 200 ms either continuously for a total of 40 s or intermittently (every 8 s) for about 3 min. When applied to the motor cortex, continuous (cTBS) and intermittent TBS (iTBS) were shown to result in depression and potentiation of cortical reactivity as indexed through suppression and facilitation of motor-evoked potentials (MEPs), respectively (Huang et al., 2005). Results of animal and human studies are consistent with the notion that the modulatory effects of TMS protocols on cortical reactivity reflect plasticity mechanisms (for review, see Cardenas-Morales et al., 2011).

2 IMPORTANCE OF PLASTICITY FOR BRAIN HEALTH ACROSS THE LIFESPAN

Plasticity is a critical component of brain development and maintenance across the lifespan. During development, brain plasticity underlies the formation of functional networks through experience-dependent strengthening and weakening of synapses. For example, animal studies have shown that whisker stimulation strengthens the development of excitatory synapses through NMDA-mediated LTP in the rat somatosensory barrel cortex (Takahashi et al., 2003). This is not seen in rats with their whiskers trimmed (Takahashi et al., 2003). Visual and auditory cortices also show

experience-dependent developmental plasticity. Repeated activation of a specific sensory input (without deprivation) potentiates neural responses to that input and is responsible for the establishment of auditory and visual receptive fields. This can be shown experimentally by exposing young rats to specific auditory stimuli that leads to enhancement of the representation of the presented frequencies and intensities in the primary auditory cortex (A1), altering auditory tuning curves and the tonotopic map (Frenkel et al., 2006; Keuroghlian and Knudsen, 2007). Similarly, presentation of high-contrast oriented gratings to young mice similarly drives orientation-specific enhancement of visual responses in the primary visual cortex (V1) (Frenkel et al., 2006).

The degree and duration of these experience-dependent changes to cortical structure are very strictly regulated. During development, there are critical periods where a specific region of cortex has heightened or exclusive capacity for plasticity. The onset of these critical periods is thought to be regulated by the maturation of specific GABAergic neurons (parvalbumin-positive basket cells) (Hensch, 2005). How these cells control plasticity is not known but may involve setting a permissive excitatory–inhibitory balance or editing pyramidal cell firing patterns to promote excitatory synaptic plasticity. The regulation of these critical periods during development and the resulting control of plasticity are integral to the healthy establishment of cortical circuits. Consequently, dysfunction of critical period timing, excitatory–inhibitory imbalance, and aberrant cortical plasticity have been put forth as potential pathophysiological mechanisms underlying developmental disorders such as autism and schizophrenia (discussed in the succeeding text) (LeBlanc and Fagiolini, 2011; Rubenstein and Merzenich, 2003).

During adolescence and adulthood, the brain continues to display capacity to adapt to the ever-changing environment, showing both functional and structural changes throughout the lifespan. For example, there is direct evidence that LTP in the hippocampus and amygdala occurs during and is required for adult learning and memory (Maren, 2005; Sossin et al., 2008). Studies have also shown that motor training in adult rats results in LTP-like strengthening of pathways within the primary motor cortex (Rioult-Pedotti et al., 2000). Similarly, presentation of temporally precise, flashed visual stimuli to adult rats alters functional synaptic connectivity and visual receptive fields in the primary visual cortex and affects visual perception in a manner consistent with induction of spike timing-dependent plasticity. In other brain regions, experience-dependent changes in synaptic strength, or synaptic plasticity, underlie many learning processes. In the reward circuit, for example, synaptic plasticity may serve as a cellular substrate for goal-directed behaviors. Addictive drugs, through a surge of dopamine released from neurons of the ventral tegmental area, induce widespread synaptic adaptations within this neuronal circuit (Bonci and Malenka, 1999; Liu et al., 2005; Luu and Malenka, 2008). It is thus proposed that drug-evoked synaptic plasticity may constitute an early cellular mechanism eventually causing compulsive drug-seeking behavior in addiction (Mameli and Luscher, 2011).

This ability to change and adapt appears to peak in young adulthood and shows a gradual but consistent decrease into senescence. Animal studies, building on

pioneering work from Barnes (Barnes, 1979; Rosenzweig and Barnes, 2003) in the late 1970s, have demonstrated an age-associated decline in synaptic plasticity in specific brain regions that correlates with neurocognitive impairments. In aged rodents, thresholds for induction of the hippocampal LTP and LTD appear to increase and decrease, respectively (Rosenzweig and Barnes, 2003). Once induced, LTP decays faster in older rats, and this appears to be associated with a greater degree of forgetfulness (Barnes and McNaughton, 1980; Kelly et al., 2006). Moreover, deficits in the balance between LTP and LTD result in impaired learning and memory (Bliss, 2003; Larson et al., 1986; Roman et al., 1987).

Direct evidence of this age-related decline in plasticity has also been shown in humans through studies using TMS measures of plasticity. For example, in a cross-sectional study of 36 healthy volunteers throughout the adult age span ranging from 19 to 81 years, Freitas et al. (2011) found the duration and magnitude of corticospinal excitability modulation by rTMS was inversely and significantly correlated with age (Fig. 1). These data provide direct experimental evidence that, in humans, LTD-like plasticity becomes increasingly less efficient with advancing age. Such decreasing plasticity in the motor cortex with advancing age may be associated with the decrement of hand motor function (e.g., longer reaction time) observed during normal aging in both men and women (e.g., Carmeli et al., 2003) and to the age-related deficits in motor learning (e.g., Brown et al., 2009). Such age-related changes in plasticity are also linked to an individual's cognitive ability and age-related cognitive decline may be associated to them. An individual's risk of age-related cognitive decline (and ultimately the manifestation of symptoms of dementia) might

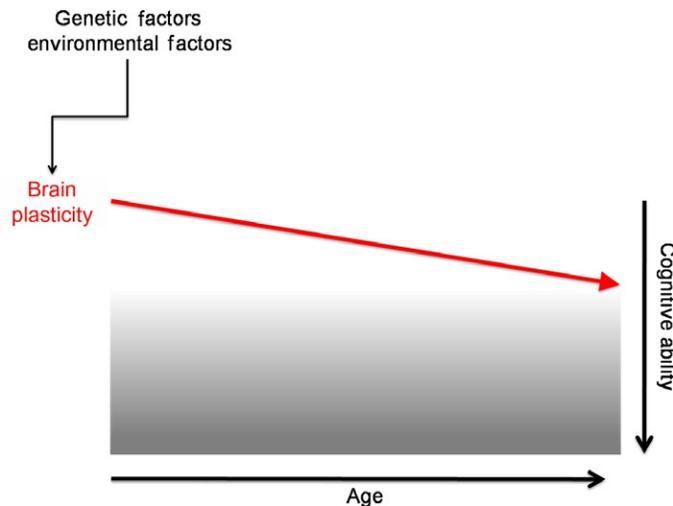


FIGURE 1

Schematic representation of the influence of aging on plasticity and cognitive ability.

then depend on the individual's starting point and slopes of change in plasticity efficiency over the lifespan. Indeed, as will be further discussed later, studies in patients with early Alzheimer's disease, the most common dementing illness, reveal an abnormally suppressed efficacy of plasticity mechanisms (Freitas et al., 2011; Koch et al., 2012).

3 DISEASE AS A MANIFESTATION OF ABERRANT PLASTICITY AT DIFFERENT TIMES IN THE LIFESPAN

If, as we suggest, plasticity is critical for healthy brain development, it follows that neuropsychological disorders may have a basis in aberrant plasticity mechanisms. Recent theories of the neurological etiology of brain disorders reflect a growing acceptance of this inference (Pascual-Leone et al., 2011; van Spronsen and Hoogenraad, 2010). A functionally "normal" brain is thus a changing brain, a brain whose capacity and mechanisms of change are shifting appropriately from one time point to another in a given individual's life. Therefore, assessing the mechanisms of brain plasticity across the lifespan is critical to gain insight into an individual's brain health. The timing, site, and direction of alterations in plasticity across the lifespan will influence what systems are affected and in turn the behavioral outcome. Important factors to consider that likely contribute to individual differences in changes in the efficacy of mechanisms of plasticity across the lifespan include genetic and epigenetic mechanisms (e.g., polymorphisms and genetic expression), hormonal factors (e.g., gender and menstrual cycle), impact of morbidities (e.g., diabetes, cancer, or infections), and lifetime experiences (e.g., traumatic brain injury, exposure to toxins, stress, sleep deprivation, substance abuse, poor cognitive reserve, poor nutrition, and sedentariness). Therefore, dissimilar "starting points" for different individuals, distinct lifelong "slopes of change," and events that lead to a change in the set point or slope of change in plasticity might be postulated (Fig. 2A and B). We shall posit that these two factors critically contribute to an individual's predisposition to manifest symptoms of disease. To illustrate this notion, we shall discuss how alterations in plasticity might underlie developmental disorders such as autism spectrum disorders (ASD) and schizophrenia and neurodegenerative disorders such as Alzheimer's disease (AD).

3.1 Autism spectrum disorders

Evidence for altered plasticity in ASD comes from multiple lines of research (reviewed in Oberman, *in press*). First, genetic linkage studies indicate that genes associated with ASD play critical roles in developmental and experience-dependent plasticity. For example, BDNF (brain-derived neurotrophic factor) plays a critical role in maintenance of synaptic potentiation (Akaneya et al., 1997; Huber et al., 1998; Jiang et al., 2001; Korte et al., 1995; Patterson et al., 1996) and has been found to be elevated in postmortem tissue of individuals with ASD, specifically in the basal

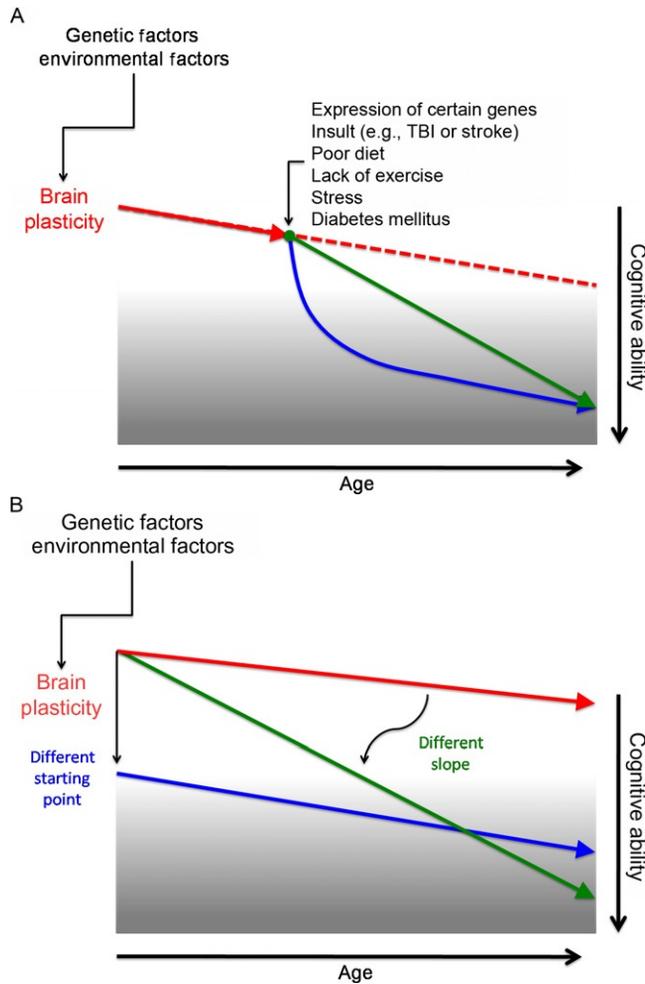


FIGURE 2

(A) Schematic representation of how factors such as expression of certain genes, diseases, brain injury, or behavior can impact the slope of change in plasticity across the lifespan. (B) Schematic representation of how degree of plasticity and cognitive ability at any given time in the lifespan is a consequence of both a given individual's starting point and slopes of change.

forebrain (Perry et al., 2001). Additionally, multiple studies note a reduction in GABAergic receptors (Fatemi et al. 2009a,b, 2010) and a 50% reduction in enzymes that synthesize GABA (glutamic acid decarboxylases (GADs) 65 and 67) (Fatemi et al., 2002; Yip et al., 2007). These changes in the GABA system may directly contribute to altered connectivity, especially between the cerebellum and the thalamus

and ultimately the cerebral cortex. This may represent a mechanism by which motor and cognitive behaviors may be affected in ASD (Blatt and Fatemi, 2011). Other genes coding for molecules such as neuroligins 3 and 4 that are implicated in synaptogenesis (Jamain et al., 2003), SH3 and multiple ankyrin repeat domains 3 (SHANK3) that encodes a protein involved in dendritic development (Durand et al., 2007) and c3orf58, sodium/hydrogen exchanger isoform 9 (NHE), and protocadherin-10 (PCDH10) thought to be critically involved in synaptic development and plasticity (Durand et al., 2007; Jamain et al., 2003; Morrow et al., 2008) have all been identified as candidate genes that confer increased risk of ASD (Cook, 2001; Lamb et al., 2000; Persico and Bourgeron, 2006).

In addition, single gene disorders associated with autism implicate proteins that play important roles in synaptic plasticity. Among these are mutations in FMRP (fragile X mental retardation protein), thought to contribute to the neurological deficits of fragile X syndrome by enhancing synaptic potentiation and favoring exaggerated LTD-like plasticity. Other examples include mutations in TSC1 and TSC2 that cause tuberous sclerosis, in NF1 that cause neurofibromatosis, and in phosphatase and tensin homolog (PTEN) that cause PTEN macrocephaly (Dolen and Bear, 2009). Although the contributions of these genes and proteins to synaptic plasticity are incompletely described, animal models of these human single gene syndromic causes of autism predictably demonstrate aberrant synaptic plasticity. These genetic findings have inspired others to propose that autism should be thought of as a “synaptopathy” (Dolen and Bear, 2009) whereby proteins that are involved in synaptic development and plasticity are affected.

Animal ASD models reveal abnormal plasticity mechanisms (reviewed in Tordjman et al., 2007). For example, a recent study exploring the parvalbumin (PV)-positive basket cell (a key player for critical period plasticity) in two animal models of autism (valproic acid (VPA) and neuroligin 3 knockout models) found a reduction or complete lack of PV cells in the parietal and occipital cortices (Gogolla et al., 2009), suggesting a possible molecular mechanism underlying a proposed hyperpotentiated state. When the microcircuits of these animals were investigated, their reactivity to stimulation, as measured by the number of spikes and the number of postsynaptic potentials following stimulation, was nearly twice that of wild-type animals (Rinaldi et al., 2008b). This hyperreactivity has been found in multiple regions including the somatosensory cortex (Rinaldi et al., 2008b), prefrontal cortex (Rinaldi et al., 2008a), and amygdala (Markram et al., 2008), thus indicating a widespread enhancement in reactivity of the cortical and subcortical neurons. Synaptic responses have also been recorded in pyramidal neurons following a Hebbian pairing stimulation protocol in these animals, and though the presynaptic response was normal, the postsynaptic cell had a more than twofold increase in response, indicating a state of hyperpotentiation (Rinaldi et al., 2007). Similarly, abnormal synaptic plasticity, specifically exaggerated LTD, has also been shown in mouse models of genetic disorders associated with autism, namely, the FMR1-null mouse (fragile X syndrome) and MECP2-null mouse (Rett syndrome) (Dani et al., 2005; Huber et al., 2002).

In humans with idiopathic autism, the most consistent neuroimaging finding is increased brain volume, with an overall increase in both gray and white matter volume (Courchesne et al., 2001). Furthermore, there is a distinct developmental trajectory of brain size abnormalities in ASD whereby reduced or normal brain size is present at birth, followed by a rapid rate of brain growth during early childhood. This trajectory suggests that the underlying mechanism is a dynamic process with a time line consistent with a shift toward increased potentiation of excitatory synapses during early childhood (Courchesne and Pierce, 2005). Recent studies reveal that the overall larger brain in individuals with ASD is primarily due to larger white matter volumes, particularly in the outer “radiate” regions including the origins and terminations of projection and sensory fibers (Herbert et al., 2004). Even when accounting for the overall greater brain volume, the proportion of white matter still is greater than normal, suggesting that abnormal axons and neural connections, rather than the neuronal cell bodies themselves, may be responsible for the abnormalities in brain structure. There is also neuropathologic data in postmortem tissue supporting brain overgrowth, specifically in the prefrontal cortex (Courchesne et al., 2011), and abnormalities at the minicolumn level indicating aberrant minicolumn structure with reduced neuronal size and increased density attributable to reductions in the inhibitory peripheral neuropil space (Casanova et al., 2002). The authors suggest that this lack of inhibition would lead to gross alterations in cortical connectivity.

Another common neuropathologic finding in ASD is a reduction in the number of cerebellar Purkinje cells (Bauman and Kemper, 1996). Such a reduction is thought to release the deep cerebellar nuclei from inhibition, producing abnormally strong physical connectivity and potentially abnormally weak computational connectivity along the cerebellothalamocortical circuit and, furthermore, possibly aberrant activity-dependent plasticity along this pathway (Belmonte et al., 2004). Abnormally high and indiscriminate physical connectivity may lead to abnormally low and ineffective functional connectivity due to excessive noise and poor temporal precision secondary to activity of superfluous connections. Consistent with this assertion, structural and functional MRI studies have confirmed anatomical and functional connectivity abnormalities in individuals with ASD (for a review, see Geschwind and Levitt, 2007).

Two recent studies have been published exploring plasticity using TMS in individuals with ASD. The first (Oberman et al., 2012) explored modulation in cortical excitability in response to a train of rTMS in 20 adults with Asperger’s syndrome (AS) and found them to have greater and longer-lasting modulation of cortical reactivity following rTMS as compared to age-, gender-, and IQ-matched controls. The latency to return to baseline following rTMS was on average between 80 and 90 min in the ASD group compared to 25–30 min in the controls. This finding was confirmed in a separate cohort of 15 individuals (Oberman et al., 2012). Interestingly, consistent with other studies, there was no significant group difference in measures of basic excitability as measured by resting and active motor threshold (Enticott et al., 2013; Oberman et al., 2012; Theoret et al., 2005) or response to single-pulse TMS (Enticott et al. 2012a; Oberman et al., 2012). Thus, this excessive modulation

of excitability in response to stimulation (a putative measure of LTD-like and LTP-like plasticity) is not primarily attributable to differences in baseline excitability. A second study was subsequently published exploring response to the PAS in nine patients with high-functioning ASD (HFA)/AS and typically developing age-matched controls. In contrast to the findings by [Oberman et al. \(2012\)](#), this study found that individuals with ASD showed a marked absence of the expected modulation of excitability following PAS ([Jung et al., 2013](#)). The authors contend that their results indicate an impairment in LTP-like plasticity induced by PAS in individuals with HFA/AS compared with typically developing participants. The conflicting findings could reflect paradigmatic differences (i.e., Hebbian vs. non-Hebbian plasticity) or the heterogeneity of ASD, but in any case, the effects are opposite (i.e., absent vs. long-lasting) and emphasize the importance of large studies, with detailed clinical and genetic information, to examine functional neurobiology in ASD. Regardless, these TMS studies support the notion of alterations in plasticity mechanisms being central to the pathophysiology of ASD.

3.2 Schizophrenia

Schizophrenia is another neurodevelopmental disorder where researchers are beginning to implicate neuroplasticity mechanisms in its pathophysiology. Several lines of evidence suggest that the neurotransmitter mechanisms mediating plasticity in the cortex are altered in schizophrenia. For example, both NMDA and GABA receptor-mediated neurotransmission have been implicated in the pathophysiology of schizophrenia. Blockade of NMDA receptor-mediated neurotransmission is associated with worsening of psychosis in patients with schizophrenia ([Krystal et al., 2002](#)) and produces behaviors in healthy subjects that are similar to the positive and negative symptoms experienced by patients with schizophrenia ([Krystal et al., 1994](#)). Moreover, neuroanatomical ([Benes and Berretta, 2001](#)) and neurophysiological evidence ([Daskalakis et al., 2002](#); [Fitzgerald et al., 2002](#); [Freedman et al., 2000](#)) suggests that both a decrease and a disruption of cortical GABAergic inhibitory neurotransmission are associated with the pathophysiological findings of schizophrenia. In addition, genetic and postmortem studies have implicated abnormalities in dysbindin, neuregulin, and reelin, proteins involved in synaptic plasticity, as possible contributors to pathological findings in schizophrenia ([Fatemi et al., 2000](#); [Stefansson et al., 2003](#); [Straub et al., 2002](#); [Weeber et al., 2002](#)).

Behaviorally, patients with schizophrenia demonstrate an inability to learn complex motor skills. For example, studies suggest that patients with schizophrenia show impaired motor learning as indexed through the rotary pursuit task and a lack of increase in blood oxygen level-dependent premotor activity following one week of training as compared to healthy subjects ([Kodama et al., 2001](#); [Schwartz et al., 1996](#)). A recent TMS study confirms these findings showing that following motor training, both medicated and unmedicated patients with schizophrenia demonstrated significantly reduced motor reorganization as indexed by TMS-induced motor-evoked potentials compared with healthy subjects ([Daskalakis et al., 2008](#)).

Several other TMS studies have been conducted that also support plasticity abnormalities in schizophrenia. [Fitzgerald et al. \(2004\)](#) showed reduced plastic brain responses in medicated and unmedicated patients with schizophrenia. Specifically, LTD-like suppression of cortical excitability was reduced in patients in response to a single 15 min train of 1 Hz rTMS applied to the motor cortex, compared with a healthy control group. [Frantseva et al. \(2008\)](#) conducted a study using PAS and demonstrated that schizophrenia patients, compared with healthy subjects, showed deficits in MEP facilitation, indicating disrupted LTP-like plasticity, which appeared to be associated with impaired motor skill learning. Finally, [McClintock et al. \(2011\)](#) reported the findings of an rTMS study in a group of six first-episode patients with schizophrenia who had 42% reduced duration of rTMS-induced aftereffects compared with age- and gender-matched healthy control subjects, suggesting that corticomotor plasticity mechanisms are already abnormally reduced in early stages of schizophrenia.

3.3 Alzheimer's disease

Large strides have been conducted in investigating the pathophysiology of AD ([Jack et al., 2010](#)). The leading hypothesis about the cause of AD argues that toxic forms of the amyloid- β ($A\beta$) protein initiate a cascade of events ending in synaptic dysfunction and cell death and where “plaques” and “tangles” are conceived as residues of this pathological process ([Mattson, 2004](#); [Walsh and Selkoe, 2004](#)). $A\beta$ is critical as when it is isolated directly from human AD brains, it can cause impaired synaptic plasticity and memory in rodents ([Shankar et al., 2008](#)). Furthermore, when $A\beta$ is released into the extracellular fluid, it triggers signaling cascades on the postsynaptic membrane, sharing remarkable similarities with LTD, including increased synaptic AMPA receptor endocytosis and dendritic spine loss ([Hsieh et al., 2006](#)).

Consistent with the clinical observation that initial symptoms of AD include memory impairment, the medial temporal lobe and other cortical structures linked to memory are affected early in AD. The reason why memory structures are particularly vulnerable to AD and critically involved in disease progression remains unclear, though proposed theories include concepts based on anatomy ([Hyman et al., 1990](#)) and on mechanisms of plasticity ([Mesulam, 2000](#)). On the other hand, early pathological studies and more recent morphometric brain studies also reveal distributed cortical regions as vulnerable to AD, prompting further exploration of systems-level causes ([Saper et al., 1987](#)). In any case, our understanding remains insufficient to guide novel interventions and current therapeutic options remain disappointing. Therefore, novel conceptualizations of AD pathogenesis seem worth entertaining.

We often consider how aberrant molecular and cellular processes can affect brain circuits and cognitive processes. However, the opposite causal direction is also possible: dysfunctional brain activity patterns may directly modulate molecular cascades that are relevant to disease. We propose that AD is an illustrative example

of this pathophysiological instance, where alterations in plasticity ultimately trigger a cascade of maladaptive responses leading to pathology.

Direct evidence of a dysfunction in plasticity in AD is provided by recent TMS studies. The first, conducted by [Inghilleri et al. \(2006\)](#), tested the effects of corticomotor modulation induced by suprathreshold high-frequency (5 Hz) rTMS and found the amplitude of MEPs progressively decreased in patients while increasing in controls. This suggests impaired LTP-like plasticity. Another study, conducted by [Battaglia et al. \(2007\)](#), studied neocortical (motor) LTP-like plasticity in AD and healthy individuals using a PAS protocol and found it to be significantly reduced in AD patients.

[Koch et al. \(2011\)](#) studied the effects of low-frequency (1 Hz) rTMS over the primary motor cortex in a group of patients with a diagnosis of probable AD, compared to healthy age-matched controls (HS), and tested the effects of a single dose of orally administered L-dopa, one of the key neurotransmitters in modulating synaptic plasticity mechanisms, on rTMS-induced plasticity. They found that in AD patients, the 1 Hz rTMS protocol did not induce the expected inhibitory effect, while a long-lasting inhibition of MEP was observed in control participants. In addition, L-dopa induced a clear form of reversal of the direction of plasticity in healthy controls that was not evident in AD. In a follow-up study, [Koch et al. \(2012\)](#) applied repetitive TMS over the primary motor cortex (M1) in AD patients and in age-matched healthy controls. Using TBS protocols, AD patients showing consistent LTD-like effects that were comparable to those obtained in healthy controls when submitted to 40 s of continuous TBS. Conversely, AD patients did not show any LTP-like aftereffect when submitted to two different TBS protocols that induced an LTP-like effect in healthy controls such as intermittent TBS and 20 s of continuous TBS followed by 1 min of muscular contraction. These results demonstrate the impairment of LTP-like together with normal LTD-like cortical plasticity in AD patients. Finally, a study conducted by [Freitas et al. \(2011\)](#) indicates that the duration and magnitude of the modulation of corticospinal excitability by cTBS, an index of LTD-like plasticity, is significantly shorter in individuals with early AD than in controls ([Freitas et al., 2011](#)). Thus, it is unclear to what extent LTD-like plasticity is affected in this population, but studies consistently reveal early alteration of mechanisms in plasticity that may antedate and contribute to trigger a molecular maladaptive cascade culminating in the manifestation of symptoms of dementia.

4 THE USE OF TMS AS A NOVEL TREATMENT STRATEGY FOR NEUROPSYCHIATRIC DISORDERS OF PLASTICITY

If, as we propose, brain plasticity is critically tied to brain health across the lifespan and a dysfunction in plasticity underlies the symptoms of many neuropsychiatric disorders, then normalizing plasticity mechanisms may represent novel and effective therapeutic interventions. In the future, interventions aimed at modulating plasticity mechanisms could potentially prevent the structural and functional pathology

underlying these disorders and in doing so prevent the behavioral symptoms from developing (Cramer et al., 2011).

The potential of rTMS to induce a long-lasting modulation of cortical excitability and plasticity offers the possibility of its use for therapeutic purposes in neurological and psychological conditions thought to be a result of altered excitability or plasticity of specific neural circuits. Studies examining behavioral performance prior to and following rTMS have shown rTMS-induced changes in sensory (Kosslyn et al., 1999), cognitive (Hilgetag et al., 2001; Mottaghy et al., 2002), and affective processing (see Lee et al., 2012 for a review). Low-frequency rTMS protocols and a specific type of theta burst stimulation (continuous, cTBS) generally induce lasting suppression of the excitability, while high-frequency rTMS and a different type of theta burst stimulation (intermittent, iTBS) generally induce lasting facilitation (Maeda et al., 2000). However, it should be noted that these effects are state-dependent and there is significant intersubject and intrasubject variability (Silvanto and Pascual-Leone, 2008). Thus, in order to induce the desired effect, one must consider (1) the brain region, as even a small shift in the targeted region may greatly affect the behavioral impact; (2) the current state of the stimulated cortex as state-dependent changes have been observed; and (3) the exact stimulation protocol being applied as opposite effects can be induced by even slight modifications of the parameters. rTMS-based treatments are already being proposed and tested in the aforementioned disorders.

4.1 Autism spectrum disorders

Recent studies from two sites in the United States (Harvard Medical School, Boston, MA, and the University of Louisville School of Medicine, Louisville, KY) and one site in Australia (Monash University, Melbourne, Australia) have reported preliminary data suggesting an improvement in both physiological indices and specific behavioral symptoms in individuals with ASD following rTMS.

The first of these studies was based on the finding that individuals with ASD showed abnormal structure of minicolumns with reduced neuronal size and increased density attributable to reductions in the inhibitory peripheral neuropil space (Casanova et al., 2002). This finding was most prominent in the prefrontal cortex (Casanova, 2006). Thus, using an rTMS protocol aimed at increasing inhibitory tone, Sokhadze et al. (2009) applied low-frequency (0.5 Hz, 150 pulses) stimulation to left dorsolateral prefrontal cortex (DLPFC) two times per week for 3 weeks in a small sample of eight individuals with ASD. The results of this first study showed an abnormally increased amplitude and latency of the P300 event-related potential (ERP) and abnormally high induced gamma frequency electroencephalographic (EEG) activity over frontal and parietal sites at baseline in the ASD group that were normalized (not significantly different from healthy controls) in amplitude and latency following the series of rTMS sessions. There was also a reduction in repetitive-ritualistic behavior in ASD subjects as reported by their caregivers. This result is quite promising, though the study should be considered extremely preliminary given

its small sample size and lack of sham control condition. Following this initial study, the same group conducted several follow-up studies with slightly larger samples. In the first of these follow-up studies, the group replicated their previous finding of normalized ERPs and a reduction in repetitive–ritualistic behaviors following the same protocol (Sokhadze et al., 2010) in 13 individuals with ASD. In the second follow-up study, the same investigators applied bilateral low-frequency TMS (1 Hz) once a week for 12 weeks, with the first six treatments to the left DLPFC and the next six to the right DLPFC in 16 patients with ASD. EEG and behavioral evaluations pre- and post-rTMS revealed normalization of induced gamma activity and a reduction in both repetitive behaviors and irritability (Baruth et al., 2010). Using this same protocol, this group explored error monitoring pre- and post-rTMS and found improvements in both ERP indices and behavioral measures of error monitoring following 1 Hz stimulation once a week first to left then to right DLPFC in 20 individuals with ASD (Sokhadze et al., 2012). Lastly, using a similar design, the same group also recently published a paper describing improvements in ERP indices of visual processing, accuracy on a selective attention task, and behavioral measures of repetitive behavior and irritability of 25 individuals with ASD following the 12-week protocol described in the preceding text (Casanova et al., 2012). Again, these studies provide promising preliminary data for the use of low-frequency rTMS to DLPFC for the alleviation of aberrant behavior and physiological indices in ASD but are limited by small sample size and unblinded designs. It is also unclear in the paradigms where both left and right hemisphere were stimulated whether the effect was driven by one or the other hemisphere or whether the effect was a result of the combination of both. Finally, the behavioral improvements appear to be limited to repetitive behaviors, irritability, and specific measures of attention.

We have also published reports showing improved performance on a behavioral task in patients with ASD following a TMS protocol. Fecteau et al. (2011) conducted a study where they applied a single session of low-frequency (1 Hz) rTMS to left and right pars triangularis and pars opercularis (the two regions that comprise Broca's area) in 10 individuals with ASD and 10 matched neurotypical control participants in a double-blind, pseudorandomized, sham-controlled study. Compared to the sham condition, all 10 individuals with ASD showed reduced latency to name objects on the Boston Naming Test following stimulation to the left pars triangularis (BA 45) while 9/10 showed an increased latency following stimulation to the adjacent left pars opercularis (BA44). The findings suggest that in individuals with ASD, left BA45 exerts an abnormally excessive amount of inhibition on left BA44, thus inhibiting left BA45 results in a suppression of the excessive inhibitory control and a behavioral improvement. However, this interpretation has yet to be empirically tested. Findings from this study though short-lived, given the single-session design, suggest that rTMS to BA45 may lead to improvements in language processing in ASD and warrant further studies aimed at long-term improvements in this domain (Fecteau et al., 2011). This study also demonstrated the importance of strict anatomical targeting as the opposite result was found when the target region was in the adjacent BA44 region.

Fitzgerald's group based in Melbourne, Australia, is also exploring the potential of rTMS to improve specific symptoms of ASD. In a recent paper, they describe a study in which a single session of 1 Hz rTMS was applied to one of two corticomotor regions (left M1 and supplementary motor area (SMA)) in 11 individuals with ASD. Though not often considered a core impairment in ASD, motor dysfunction is often noted as an associated feature. Following stimulation of M1, there was a significant improvement in a late movement-related cortical potential (MRCP) thought to be associated with the execution of movement while stimulation of SMA resulted in an improvement of the early MRCP, suggesting enhanced motor preparation. Though poststimulation improvements were seen, their MRCPs still remained outside of what would be considered neurotypical levels, and despite improvements in the electrophysiological response, there was not a significant improvement in behavioral measures of motor functioning (Enticott et al., 2012b).

This same group is currently conducting a sham-controlled, double-blind clinical trial of a specific type of high-frequency rTMS (deep rTMS) to the medial prefrontal cortex (mPFC), a region thought to play a key role in theory of mind abilities (understanding the mental state of others) (Amodio and Frith, 2006; Frith and Frith, 1999; Mitchell et al., 2006; Saxe and Powell, 2006). The goal of this study is to develop a therapeutic intervention aimed at improving the individual's capacity for understanding other's mental states. Though this study is still ongoing, the group has reported that several participants have responded to the treatment resulting in a reduction of self-reported clinical symptoms (Enticott, personal communication). An individual who had a very pronounced response (Ms. D) was featured in a case report (Enticott et al., 2011). This patient showed improvements on the Interpersonal Reactivity Index (IRI), the Autism Spectrum Quotient (AQ), and the Ritvo Autism–Asperger Diagnostic Scale. She also reported that she found eye contact “less uncomfortable” and found social situations “more natural” even joining a social club and making new friends. She noted that she “did not have to think so much of what to say” and was more aware of instances when she might be making someone uncomfortable. She also reported an increased capacity for empathy and perspective taking, even for incidents that occurred many years before. She also experienced greater consideration for and affection toward family members following the stimulation protocol. These changes were also noted by her family. Her mother described her as more considerate of others following the stimulation. These improvements seemed to remain at the 1-month and 6-month follow-up (Enticott et al., 2011). Still, other groups including one in Israel (NCT 01388179) and one in France (NCT 01648868) also have ongoing clinical trials applying rTMS for the treatment of specific ASD symptoms, the results of which have yet to be published.

4.2 Schizophrenia

Studies using TMS and rTMS in schizophrenia have been more extensively reviewed in Freitas et al. (2009). Initial rTMS studies focused on the clinical efficacy of rTMS on the positive and negative symptoms of the disease, but overall, the results were

inconsistent and effect sizes rather small. For positive symptoms (specifically auditory hallucinations), the goal was to inhibit the left temporoparietal cortex via 1 Hz rTMS, based on the rationale that increased temporal activity correlates with positive symptoms (for a review, see Freitas et al., 2009). In regard to negative symptoms, numerous studies attempted to increase the activity in the left prefrontal region via high-frequency rTMS as this might regulate the dopamine release and ameliorate the negative symptoms.

Among numerous studies that targeted the negative symptoms, only five randomized controlled trials assessed the cognitive effects (Fitzgerald et al., 2008; Mittrach et al., 2010; Mogg et al., 2007; Novak et al., 2006; Schneider et al., 2008). Mogg et al. applied 10 consecutive daily sessions of 10 Hz rTMS to the left DLPFC and reported a significant improvement in verbal learning in a series of patients with prominent negative symptoms. In addition, two intraindividual crossover studies applied 10 sessions of 20 Hz rTMS to the left DLPFC (Huber et al., 2003; Rollnik et al., 2000), and though initially failed to detect a significant effect of rTMS on cognition (Rollnik et al., 2000), when analyzed stratifying for gender, an improvement of visuomotor tracking was observed in females (Huber et al., 2003).

Further studies seem warranted, specifically considering the encouraging findings of open, proof-of-principle trials. For example, Cohen et al. (1999) stimulated the PFC bilaterally with 20 Hz using a double-cone coil, a special coil considered to stimulate deeper brain regions compared to standard figure-of-eight coil. Following 10 sessions of rTMS, the authors reported an improvement in visual memory. In a recent study, Levkovitz et al. (2011) performed bilateral deeper stimulation of the prefrontal cortex (L > R) using an H-coil and reported improvement in executive functions, spatial working memory, attention, and rapid visual information processing. It seems that indeed the use of special TMS coils that enable direct stimulation of deeper brain structures may be important in this setting. Studies using more conventional TMS coils with limited depth penetrance have yielded less encouraging results. For example, Sachdev et al. applied 20 sessions of 20 Hz rTMS to the left DLPFC and found no improvement in cognitive functions (Sachdev et al., 2005).

Another promising approach in schizophrenia appears to be the targeting of nodes of identified neural networks. Specifically, targeting cerebellar vermis to have an impact of distributed bihemispheric neural networks is an intriguing notion (Demirtas-Tatlidede et al., 2011). Schutter et al. (2003) reported early promising results targeting the cerebellar vermis. In a carefully designed open-safety study, we embraced this novel approach and targeted the cerebellar vermis using an intermittent TBS paradigm (Demirtas-Tatlidede et al., 2010). Following 10 sessions of stimulation in 5 days (twice per day with a minimum gap of 4 h), we observed an improvement in working memory and visual learning domains while no significant decline was found. The direction of improvement in 70% of the neuropsychological variables suggests a trend toward improvement in cognition. A double-blind, sham-controlled phase II study is currently underway.

Another important consideration in this setting is the possibility of employing stimulation paradigms tuned to specific brain oscillations and targeting

bihemispheric structures. The combination of TMS with EEG and specifically EEG-gated TMS protocols enables such approaches (Shafi et al., 2012). For example, rTMS can lower the excessive gamma oscillatory activity found in patients with schizophrenia when applied at appropriate stimulation frequency bilaterally over the DLPFC (Barr et al., 2011). This was associated with significant improvements in working memory.

4.3 Alzheimer's disease

We hypothesize that a therapy that targets specific brain circuits that are impaired in AD in order to promote their functional integrity and restore their plasticity might preserve cognitive function and effectively reduce the burden of the disease. Data from several small, single-site, randomized controlled trials reveal extremely encouraging results. If confirmed in appropriately powered and controlled clinical efficacy trials, such an approach would represent a major advance in the treatment of AD that could be truly transformative for the care of patients, reducing the impact on their families and potentially producing a substantial financial saving for society. Furthermore, such an approach might serve as a proof-of-concept for the notion of harnessing and modulating plasticity as a cornerstone of neurological therapeutics.

The hypothesis underlying the proposed novel therapeutic approach is that repetitive TMS targeting specific nodes of brain networks affected in AD can enhance plasticity and modulate connectivity in the targeted brain circuit, thus making it more responsive to circuit-specific CR tasks and altering the pathological metabolic cascade.

Two randomized controlled trials have been published using TMS for AD and both reported positive changes following consecutive sessions of rTMS application.

Cotelli et al. (2011) applied 20 sessions of 20 Hz rTMS over the left DLPFC and performed a series of language tests in patients with moderate AD. The authors reported a significant effect of rTMS on auditory comprehension. Secondly, Ahmed et al. (2012) tested the effects high- and low-frequency rTMS applied over the bilateral DLPFCs. A significant improvement in global cognitive functioning was reported following five consecutive sessions of bilateral high-frequency stimulation and this effect was maintained for 3 months.

In an open trial, Bentwich et al. (2011) tested the effects of 10 Hz rTMS together with cognitive training in patients with AD. This combined therapy was applied for 6 weeks while the authors stimulated six different locations (Broca, Wernicke, right and left DLPFCs, and right and left parietal somatosensory association cortices) with an aim to cover the cognitive domains affected by the disease. A significant improvement in the primary outcome measure, Alzheimer Disease Assessment Scale-Cognitive (ADAS-cog), was detected at 6 weeks and 4.5 months. MMSE revealed a significant change at 6 weeks only.

Subsequently, Rabey et al. (2013) completed a small, randomized double-blind controlled study of TMS-CR in 15 patients with mild-moderate AD on

cholinesterase inhibitor therapy (stable dose for ≥ 2 months). Seven patients were randomized to TMS-CR while eight were double sham controls. They followed exactly the same protocol as our pilot study and found a mean improvement on the ADAS-cog of 3.8 points in the active TMS-CR group, as compared with a mean improvement of 0.5 in the control group ($p = 0.04$, mean difference in ADAS-cog between groups at endpoint of 4.3 points). There was also a significant improvement in the average CGIC score in the real versus sham groups ($p < 0.05$): the CGIC is a 7-point “global change” rating in which 4 = no change and 3, 2, and 1 or 5, 6, and 7 is “minimal,” “moderate,” and “marked” improvement or worsening, respectively. The real TMS-CR group showed an average change rating of 3.6 and the sham group an average change rating of 4.3, representing slight average improvement and worsening, respectively. The difference between means, in this case 0.7, is what represents the degree of difference between treatments in global change. This mean difference compares favorably to the one encountered in trials of marketed treatments, which has been in the 0.3–0.4 range. There were no reported side effects of treatment. A double-blind, multiple site European study is under way to confirm these promising findings.

We have recently completed an investigator-initiated randomized, double-blind clinical trial in 12 patients with mild–moderate AD (MMSE 18–26). Patients were randomized to active ($n = 6$) or sham ($n = 6$) intervention. Patients underwent 6 weeks of daily 1 h sessions of active or sham TMS-CR as adjunct to their stable pharmacological therapy (five sessions per week, Monday to Friday, total of 30 sessions). A short train of repetitive TMS was applied to a given brain region immediately before cognitive training tailored to engage the targeted brain circuit. Six different brain regions engaged in major cognitive functions affected by AD were targeted, as identified using the patient’s own brain MRI scan. The cognitive tasks were developed to fit these regions and engaged the modulated brain circuits. The primary outcome measure was to assess improvement relative to sham on the ADAS-cog score at the end of the 6 weeks of intervention and at a 3-month follow-up. The active treatment group improved by 2.9 points relative to baseline, whereas the sham treatment group worsened by 2.7 points ($p < 0.01$). Therefore, a primary analysis for the difference between groups at endpoint, controlling for baseline (effectively a covariance analysis or a test of difference scores), revealed a mean difference in ADAS-cog between groups at endpoint of 5.6 points, markedly greater than the reported effect of pharmacological or nonpharmacological interventions. It is further compelling that relative to baseline, *all* patients in the active TMS-CR group showed an improvement (either immediately after the intervention or within 1 month), while none of the patients in the sham group showed improvement.

The few trials conducted to date reveal positive effects and provide initial evidence on the potential of noninvasive brain stimulation for cognitive enhancement in AD. However, these studies have not been replicated and the evidence remains preliminary. While the initial target in patients with mild cognitive impairment and mild AD should be to halt the progression of the disease, cognitive enhancement strategies in moderate to severe AD should target multiple cognitive domains in

conjunction with cognitive training in order to achieve a clinically meaningful effect. Further systematically designed, sham-controlled trials will establish whether non-invasive brain stimulation might prove an effective cognitive-enhancing strategy for this implacable disease.

5 CONCLUSION

The brain changes across the lifespan. First, growing evidence demonstrates that the brain undergoes a complex array of neuroanatomical and neurophysiological modifications from birth till death, so that concepts such as “development” and “senescence” have become increasingly arbitrary in their definition. Instead, the lifespan and the aging process itself might be best viewed as a “lifelong developmental process,” which is thought to constitute the underpinnings of shifts in cognition and behavior throughout each individual’s life. Second, along with changes in brain structure and function, the mechanisms by which structure and function can be modified (the mechanisms of brain plasticity themselves) appear to also change over the lifespan. This developmental process is very well controlled by the processes described in the preceding text including LTP, LTD, and homeostatic and metaplastic control of these processes. Over the course of development, the brain goes through critical periods where a specific region of cortex has heightened or exclusive capacity for plasticity.

This chapter highlights the importance of brain plasticity throughout the lifespan for optimal brain health. In health, local cortical and network plasticity might keep a fine-tuned balance, which optimizes functionality (Pascual-Leone et al., 2011). Such a “lifelong dynamic, plastically changing brain” poses several challenges, including the definition of a functionally “normal” brain at a given point in time in a given individual. A functionally “normal” brain is a changing brain, a brain whose capacity and mechanisms of change are shifting appropriately from one time point in life to another.

We have also highlighted how pathology of brain plasticity may underlie a number of neuropsychological disorders across the lifespan. ASD and schizophrenia may represent two sides of the same coin with the symptoms of ASD potentially stemming from uncontrolled excitatory plasticity and an overall potentiated cortex and symptoms of schizophrenia stemming from a lack of excitatory plasticity. At the other end of the lifespan, in late adulthood, maintaining the capacity for plastic change may be critical for avoiding age-related cognitive decline with dementia and AD representing an inability for plastic change.

If, as we propose, these diseases and disorders stem from aberrant plasticity mechanisms, then modulating such systems using TMS may represent a novel alternative to drug treatments. Pilot studies suggest promise for the treatment of ASD, schizophrenia, and AD using specific rTMS protocols. As of now, these treatments should be considered highly experimental and in need for further replication in properly powered and controlled trials. However, they offer valuable proof-of-principle support for the concept of harnessing and guiding brain plasticity for neurotherapeutics.

The future of translational neuroscience with the ultimate goal of understanding the mechanisms driving brain health and disease and developing therapeutic interventions that optimally treat brain diseases depends on our ability to (1) understand the mechanisms of plasticity across the lifespan and how they are optimized in neurologically healthy individuals, (2) identify how dysfunction in these mechanisms can account for the clinical phenotype of neuropsychological diseases across the lifespan, and finally (3) further develop approaches and tools to (ideally noninvasively) treat disorders of brain plasticity. If one assumes that abnormalities in plasticity predate any structural or functional brain alterations or any behavioral symptom, then therapeutic approaches to normalize brain plasticity may reduce or prevent the anatomical and functional brain pathology underlying these disorders and in doing so prevent the clinical manifestation of the disease.

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